

Convolutional neural network with binary moth flame optimization for emotion detection in electroencephalogram

Tabarek Alwan Tuib¹, Baydaa Hadi Saoudi², Yaqdhan Mahmood Hussein¹, Thulfiqar H. Mandeel³,
Fahad Taha Al-Dhief⁴

¹College of Engineering Electronics and Communication Engineering, Al Muthanna University, Samawah, Iraq

²Department of ICT, Al-Samawa Technical Institute, Al-Furat Al-Awsat Technical University, Nafaq, Iraq

³Department of Computer Techniques Engineering, College of Information Technology, Imam Ja'afar Al-Sadiq University, Baghdad, Iraq

⁴School of Electrical Engineering, Faculty of Engineering, Universiti Teknologi Malaysia, UTM Johor Bahru, Johor, Malaysia

Article Info

Article history:

Received Nov 26, 2022

Revised May 28, 2023

Accepted Jun 30, 2023

Keywords:

Binary moth flame optimization

Classification

Convolutional neural networks

Electroencephalogram signals

Emotion detection

ABSTRACT

Electroencephalograph (EEG) signals have the ability of real-time reflecting brain activities. Utilizing the EEG signal for analyzing human emotional states is a common study. The EEG signals of the emotions aren't distinctive and it is different from one person to another as every one of them has different emotional responses to same stimuli. Which is why, the signals of the EEG are subject dependent and proven to be effective for the subject dependent detection of the Emotions. For the purpose of achieving enhanced accuracy and high true positive rate, the suggested system proposed a binary moth flame optimization (BMFO) algorithm for the process of feature selection and convolutional neural networks (CNNs) for classifications. In this proposal, optimum features are chosen with the use of accuracy as objective function. Ultimately, optimally chosen features are classified after that with the use of a CNN for the purpose of discriminating different emotion states.

This is an open access article under the [CC BY-SA](#) license.



Corresponding Author:

Tabarek Alwan tuib

College of Engineering Electronics and Communication Engineering, Al Muthanna University

Samawah, Iraq

Email: tabarcka@gmail.com

1. INTRODUCTION

Brain-computer interfaces (BCI) are devices allowing the users to mentally manage a computer program or Neuro prosthesis by translating brain activity into sequences of commands for the computer [1]. Human computer interaction became part of the daily life. In a similar way, the emotions are significant and they constantly exist in the daily lives of the people. Emotions could provide numerous prospects in the enhancement of interactions with the emotion-based computers, for example, the affective interactions for the epileptic or autistic patients [2] It facilitates communication, particularly for physically challenged individuals [3]. Emotions have an important impact on many tasks, including decision making, communication, and human-computer interactions [4]. Emotion is a type of the unconscious or conscious feeling for a work or phenomenon. Emotions are expressed by a variety of the physical and biological reactions, which include text, voice, gestures, bio signals and facial expressions.

The people can't hide their emotions although they do not want to show them. The reactions to the emotions are a very significant key for communications amongst people [5] the detection of the emotions represents one of the very important sub-areas of the affective computing, focusing upon the recognition of the human emotions that are based upon various modalities, such body language, audio-visual expression,

physiological signals, and so on. In comparison with other Emotion detection is a significant affective computing sub-area, focusing on the recognition of the human sentiments based upon various modalities, like physiological signals, body language, audio-visual expressions, and so on. In comparison with other modalities, physiological signals, like the EEG, electromyography (EMG), electrocardiogram (ECG), galvanic skin response (GSR), and so on, have a benefit of being hard to disguise or conceal [6]. Compared to other outward appearance indicators like the facial expression and gesture, the method based on EEG data is more dependable among numerous approaches to emotion identification due to its objective evaluation and high accuracy [7]. There are several techniques for detecting brain activity, including magnetic resonance imaging (MRI) [8], [9] magnetoencephalography (MEG) [10]. Off grid communication has been implementation in [11] and electroencephalogram [12].

However, because the EEG has a quick reaction time and is less costly than other techniques, it is commonly employed to monitor brain activity in brain-computer interfaces (BCI) research [12], [13]. By inserting electrodes on the scalp, the EEG signals are captured as a weak potential and analyzed to create a BCI system. The study has been based upon the recording and analyses of EEG brain activity, as well as the recognition of EEG patterns linked with mental states [14]. Several strategies for designing a BCI system based on EEG signals have been proposed, including event-related synchronizations [15] and event-related desynchronization [16]. A variety of EEG-based BCI systems were lately created in which feature extraction and classification algorithms may identify EEG patterns in different mental states for information transmission [17].

Understanding brain's reactions to the variety of the emotional states could considerably develop the computer models for the identification of the emotions. Numerous psychophysiology investigations [18]–[20] showed relationships between human emotions and EEG patterns. In addition to that, with rapid development of wearable devices and dry electrode approaches [21]–[24], there is now a possibility to transfer EEG-based emotion recognitions from the laboratory to the real-world applications like the driving fatigue detections and monitoring of the mental states [25]–[29].

Convolutional neural networks (CNNs) are a type of end-to-end model. End-to-end models that are based upon the deep neural networks (DNNs) learn to map effectively from the main input to expected output through the DNN. This prevents design and selections of complex manual features. However, utilizing the CNNs for detecting the EEG emotions cannot directly accomplish the ideal results. The reason for this is that the order of the input channels entering the CNNs must be meaningful. None-the-less, the main EEG channels aren't sorted according to their features. Channel proximity does not indicate the amount of channel information. Which is why, the strategy of the increase of the amount of the information in the adjacent channels through adjusting the channels one more time helps CNNs to learn effectively [30].

When the number of classified emotions is increased, the accuracy of EEG-based emotion detection system is decreased. Since EEG contains noise and artifacts, emotion detection by EEG is still challenging. In this paper, authors paid attention to emotion detection in EEG signals based of a binary moth flame optimization (BMFO) algorithm for feature selection and CNN for classifications. In this proposed study, optimum features have been selected with the use of the accuracy as objective function. Finally, optimally chosen features will be classified after that with the use of the CNN for discriminating different emotion states.

2. PROPOSED METHOD

The emotion may be recognized mainly with a variety of the modalities such as the face images, gestures and speech. Nonetheless, those methods of recognition have a susceptibility to person's age, language, culture, habit and appearance, which is why, they're not universal and they lack the accuracy of the recognition. In the present paper, the focus has been directed towards the recognition of emotions and connectivity analyses with the CNNs. The suggested approach has 3 stages. In pre-processing stage, independent component analysis (ICA) approach was used for removal of noise that is fundamentally induced electroencephalogram (EEG), signals. For the purpose of achieving enhanced accuracy and high true positive rate the suggested system introduced a binary moth-flame optimization (BMFO) [31] for feature selection and CNN for classification as can see Figure 1. The emotion recognition performed by CNN with subject-independent connection features. CNN can be defined as an End-to-End model type. End-to-end models that are based upon DNN effectively learn mapping from original inputs to expected outputs via DNN. It avoids complicated manual feature design and selections. However, directly utilizing the CNNs in the EEG emotion recognitions could barely accomplish optimal results. It is because the channels' order of inputs that are fed into the CNNs must be meaningful. None-the-less, original EEG channels' orders aren't arranged based their characteristics. The channels' proximity doesn't reflect relevant information value between channels. Which is why, the strategy of the increase of information amount on the adjacent channels through the rearrangements of the channels will help the CNNs to learn in a more effective way. In the meantime, the features of the Pearson correlation coefficient could be representing information of the connectivity between the variety of the channels of the EEG signal.

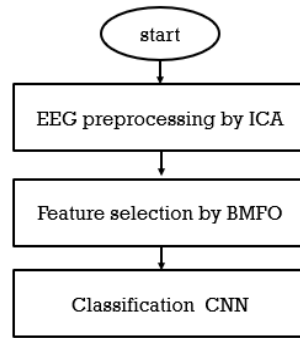


Figure 1. The flowchart of the classifications of the emotional states from the EEG data

2.1. Feature selection by BMFO algorithm

The moth flame optimization (MFO), which has been suggested by S. Mirjalili in 2015 [32], can be defined as a new algorithm of optimization that has been inspired by moths' special navigation approach in the nature, which is referred to as the transverse orientation. The moths can be considered as fancy insects, attracting towards an artificial light or the moonlight. Based on the MFO algorithm, the main MFO algorithm moth modules (i.e., the actual search agents) and flames (i.e., optimal moth position). The distinct moth position is updated based on the flame based on [31]. M_i can given in (1):

$$M_i = S(M_i, F_j) = D_i * e^{bt} * \cos(2\pi t) + F_j \quad (1)$$

where M_i represents i th moth, S represents logarithmic spiral function, F_j denotes j th flame, D_i represents distance from M_i to F_j , b represents a constant value that defines logarithmic spiral shape and t represents some random number in $[-1, 1]$. For the binary search space, moth positions are limited to binary variable. Which is why, a sigmoidal function has been utilized for the purpose of transforming the position of every one of the moths updated based on a flame (1) into the new position in the binary search space (2) for the BMFO.

$$M_i = \begin{cases} 1 & \text{if } r \text{ and } < \frac{1}{1+e^{-(X(I+1))}} \\ 0 & \text{otherwise} \end{cases} \quad (2)$$

Where $X(I+1)$ represents real-value location update of moth for $(I+1)$ th iteration and rand represents some random number which is chosen in the $(0, 1)$ interval.

3. EVALUATION

3.1. Data-set

The data-set that has been used in the experimentations is Shanghai Jiao Tong University (SJTU) emotion data-base [33], containing 15 subjects' EEG data (8 females + 7 males). In this data-set, EEG signals have been recorded with the use of a 64 channel AgCl electrode at a 1,000 Hz sampling rate with the use of international 10–20 system. Every electrode's impedance has been $< 5k\Omega$. SEED data-set was denoised by a band pass filter and artefacts removal approach. And those denoised EEG signals have been divided to 5 brain waves that correspond to frequency bands for all of the 62 channels. After that, brain waves have been separated to 1 sec. fragments and DE features have been extracted. Based on the theory that higher bands of frequency like β are more powerful and crucial in the detection of the EEG emotions. Figure 2 shows an example of binaural and noise signals.

3.2. The initialization of parameters

For checking the quality of the suggested algorithm, we adjusted CNN parameters. We did this task by considering 30 for maximum iteration, training percentage was considered for 80% of the data, and test percentage was taken into account for 20% of the data. Table 1 shows the settings of the parameters (CNN).

3.3. The evaluation criteria

The choice of criterion for evaluating the efficiency of the approach is dependent upon the problem that needs being solved. We assume that some data samples are available. These data are given separately to

the model and a class is received as output for every one of them. The predicted class of the model and the actual class of data have been listed in a Table 2 that has been referred to as the confusion matrix.

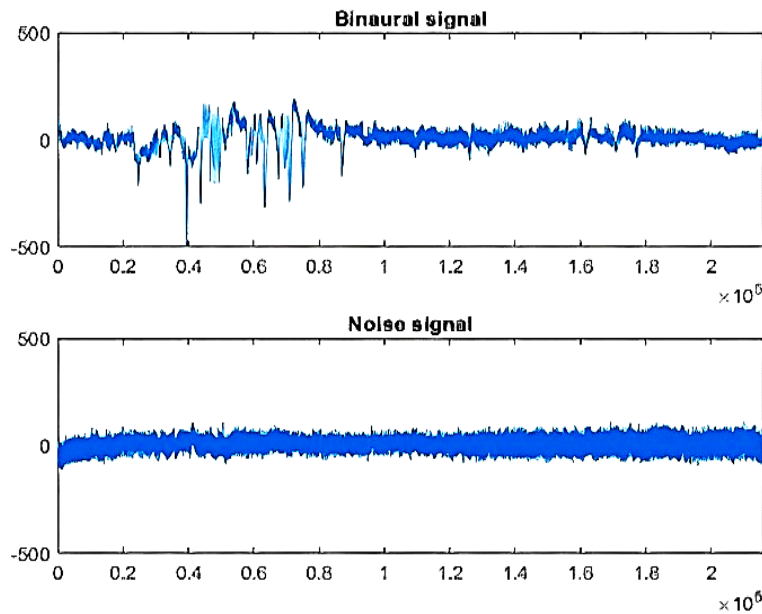


Figure 2. Plot of binaural and noise signals

Table 1. Initial values for parameters on CNN

Parameter	Initial parameters
Maximum iteration	30
Training percentage	80%
Test percentage	20%
Input layers	[64,128,1]
Learning rate	0.001

Table 2. Confusion matrix

	P	N	
PP Predicted positives	TP True positives	FP False positives	$\frac{TP}{PP}$ precision
PN Negative predictions	FN False negatives	TN True negatives	
	$\frac{TP}{P}$ Recall/sensitivity	$\frac{TN}{N}$ feature	

Section, it provides an exact description and definition of the confusion matrix. From this table, four simple criteria can be obtained directly: TP (i.e., true positive) and TN (i.e., true negative) denote the number of the positive and negative samples which have been accurately classified, while FP (false positive) and FN (false negative) are the number of the positive and negative samples which have been incorrectly classified,

- True positive rate: TPR (true positive rate) = $TP/(TP+FN)$. Rate of the positive samples that are correctly classified in positive class. It is also called a recall or sensitivity.
- True negative rate: TNR (correct negative rate) = $TN/(FP+TN)$. Rate of the negative samples that are correctly classified in the negative class are also called feature.
- False Positive Rate: FPR (false positive rate) = $FP/(FP+TN)$. Rate of the negative samples that are incorrectly classified in the negative class.
- False negative rate: FNR (false negative rate) = $FN/(TP+FN)$. Percentage of the positive samples that are incorrectly classified in the negative class.

3.3.1. Accuracy criterion

The most common criterion for classifying accuracy and vice versa is the error rate. This one is the ratio of positive samples that are actually positive and shows the accuracy of the learning model. Mathematically, this ratio can be described in (3),

$$Accuracy = \frac{TP+TN}{TP+FP+FN+TN} \quad (3)$$

3.4. The evaluation of results

Emotions are characterized by the EEG signal with a variety of the feature extraction approaches and classification algorithms. The accuracy of the emotions could vary from one extract method to the other. After the implementation of the proposed approach in MATLAB 2018b environment and using the sama plot program, the results of both accuracy and detection rate were plotted, and the sorted results from the proposed improved neural network are shown in Table 3. CNN, have been compared. We compared the accuracy of current and proposed approaches for discriminatory emotion state. Compared with the existing methods, the error rate is reduced and the accuracy is superior to the existing approaches. In addition, the proposed network structure is simple and the memory consumption parameters are few. We also confirm that the shallow network also has a relatively good detection effect. In Figures 3 and 4, the trend of increasing accuracy and decreasing losses over 50 epochs.

Table 3. The comparison accuracy results of the suggested approach with the level of various techniques

S.no	Feature Selection	Classify method	Accuracy
1	BMFO	CNN	99.4%
2	Firefly Algorithm	ISO-FLANN Classification	95 %
3	DWT	K-NN	83.26%
4	Dynamic features and PCA	SVMs	64.70 _ 82.91%
5	WT	SVMs	82.38 %
6	HOC	SVMs	82.33%
7	STFT	SVMs	80%
8	HOC	NN	80.50%
9	Connectivity Features And PCA	RBF	84.60%
10	DWT	LDA	75.21 %
11	HOC	QDY	62.3 %

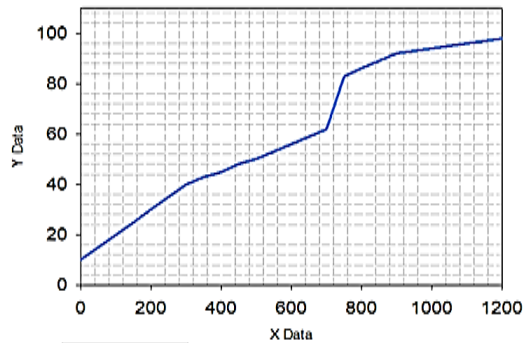


Figure 3. The accuracy results of the proposed approach during 50 epochs

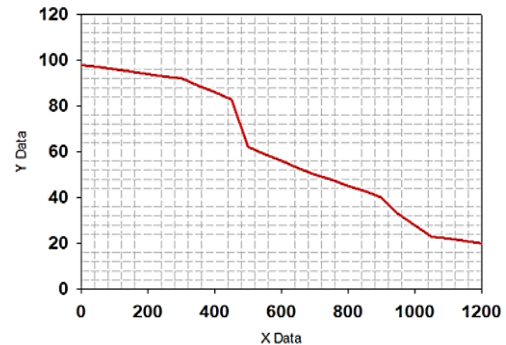


Figure 4. The loss results of the proposed approach during 50 epochs

4. CONCLUSION

We introduced emotion recognition based on EEG algorithm. In this algorithm, emotion is associated with the EEG signals. were the proposed system introduced a binary moth flame optimization (BMFO) algorithm for feature selection and convolutional neural networks (CNN) for classification. In the suggested study, optimum features had been chosen with the use of the accuracy as objective function. Finally, optimally chosen features will be classified after that with the use of a CNN for discriminating a variety of the states of emotions. We compared the accuracy of current and suggested approaches for discriminatory emotion state. Compared with the existing methods, the error rate is reduced and the accuracy is better than the existing approaches. In addition, the suggested network structure is simple and the memory consumption parameters are few.

REFERENCES




- [1] S. Nasehi and H. Pourghassem, "A new feature dimensionally reduction approach based on general tensor discriminant analysis in EEG signal classification," in *Proceedings - 2011 International Conference on Intelligent Computation and Bio-Medical Instrumentation, ICBMI 2011*, Dec. 2011, pp. 188–191. doi: 10.1109/ICBMI.2011.32.
- [2] R. M. Mehmood and H. J. Lee, "EEG based emotion recognition from human brain using Hjorth parameters and SVM," *International Journal of Bio-Science and Bio-Technology*, vol. 7, no. 3, pp. 23–32, Jun. 2015, doi: 10.14257/ijbsbt.2015.7.3.03.
- [3] A. Walendziak, "Nontrivial BCK/BCI-algebras do not satisfy the fuzzy ascending chain condition," *Fuzzy Sets and Systems*, vol. 158, no. 8, pp. 922–923, Apr. 2007, doi: 10.1016/j.fss.2006.11.018.
- [4] M. Murugappan, N. Ramachandran, and Y. Sazali, "Classification of human emotion from EEG using discrete wavelet transform," *Journal of Biomedical Science and Engineering*, vol. 03, no. 04, pp. 390–396, 2010, doi: 10.4236/jbise.2010.34054.
- [5] H. Yang, J. Han, and K. Min, "A multi-column CNN model for emotion recognition from EEG signals," *Sensors (Switzerland)*, vol. 19, no. 21, p. 4736, Oct. 2019, doi: 10.3390/s19214736.
- [6] P. Zhong, D. Wang, and C. Miao, "EEG-based emotion recognition using regularized graph neural networks," *IEEE Transactions on Affective Computing*, vol. 13, no. 3, pp. 1290–1301, Jul. 2022, doi: 10.1109/TAFFC.2020.2994159.
- [7] F. T. Al-Dhief *et al.*, "Voice Pathology detection using machine learning technique," in *2020 IEEE 5th International Symposium on Telecommunication Technologies, ISTT 2020 - Proceedings*, Nov. 2020, pp. 99–104. doi: 10.1109/ISTT50966.2020.9279346.
- [8] I. Prohovnik, P. Skudlarski, R. K. Fulbright, J. C. Gore, and B. E. Wexler, "Functional MRI changes before and after onset of reported emotions," *Psychiatry Research - Neuroimaging*, vol. 132, no. 3, pp. 239–250, Dec. 2004, doi: 10.1016/j.psychres.2004.03.005.
- [9] J. Zhang, G. Sudre, X. Li, W. Wang, D. J. Weber, and A. Bagic, "Clustering linear discriminant analysis for MEG-based brain computer interfaces," *IEEE Transactions on Neural Systems and Rehabilitation Engineering*, vol. 19, no. 3, pp. 221–231, Jun. 2011, doi: 10.1109/TNSRE.2011.2116125.
- [10] A. S. Garrett and R. J. Maddock, "Separating subjective emotion from the perception of emotion-inducing stimuli: An fMRI study," *NeuroImage*, vol. 33, no. 1, pp. 263–274, Oct. 2006, doi: 10.1016/j.neuroimage.2006.05.024.
- [11] Y. M. Hussain *et al.*, "Smartphone's off grid communication network by using Arduino microcontroller and microstrip antenna," *Telkomnika (Telecommunication Computing Electronics and Control)*, vol. 19, no. 4, pp. 1100–1106, Aug. 2021, doi: 10.12928/TELKOMNIKA.v19i4.15949.
- [12] C. Guger *et al.*, "How many people are able to control a P300-based brain-computer interface (BCI)?," *Neuroscience Letters*, vol. 462, no. 1, pp. 94–98, Sep. 2009, doi: 10.1016/j.neulet.2009.06.045.
- [13] S. Nasehi and H. Pourghassem, "Online mental task classification based on DWT-PCA features and probabilistic neural network," *International Journal of Imaging and Robotics*, vol. 7, no. 1, pp. 110–118, 2012.
- [14] H. J. Hwang, K. Kwon, and C. H. Im, "Neurofeedback-based motor imagery training for brain-computer interface (BCI)," *Journal of Neuroscience Methods*, vol. 179, no. 1, pp. 150–156, Apr. 2009, doi: 10.1016/j.jneumeth.2009.01.015.
- [15] L. Leocani *et al.*, "Movement preparation is affected by tissue damage in multiple sclerosis: Evidence from EEG event-related desynchronization," *Clinical Neurophysiology*, vol. 116, no. 7, pp. 1515–1519, Jul. 2005, doi: 10.1016/j.clinph.2005.02.026.
- [16] L. I. Aftanas, A. A. Varlamov, N. V. Reva, and S. V. Pavlov, "Disruption of early event-related theta synchronization of human EEG in alexithymics viewing affective pictures," *Neuroscience Letters*, vol. 340, no. 1, pp. 57–60, Apr. 2003, doi: 10.1016/S0304-3940(03)00070-3.
- [17] D. Coyle, T. M. McGinnity, and G. Prasad, "Improving the separability of multiple EEG features for a BCI by neural-time-series-prediction-preprocessing," *Biomedical Signal Processing and Control*, vol. 5, no. 3, pp. 196–204, Jul. 2010, doi: 10.1016/j.bspc.2010.03.004.
- [18] D. Sammler, M. Grigutsch, T. Fritz, and S. Koelsch, "Music and emotion: Electrophysiological correlates of the processing of pleasant and unpleasant music," *Psychophysiology*, vol. 44, no. 2, pp. 293–304, Mar. 2007, doi: 10.1111/j.1469-8986.2007.00497.x.
- [19] G. G. Knyazev, J. Y. Slobodskoj-Plusnin, and A. V. Bocharov, "Gender differences in implicit and explicit processing of emotional facial expressions as revealed by event related theta synchronization," *Emotion*, vol. 10, no. 5, pp. 678–687, Oct. 2010, doi: 10.1037/a0019175.
- [20] D. Mathersul, L. M. Williams, P. J. Hopkinson, and A. H. Kemp, "Investigating models of affect: Relationships among EEG alpha asymmetry, depression, and anxiety," *Emotion*, vol. 8, no. 4, pp. 560–572, 2008, doi: 10.1037/a0012811.
- [21] C. Grozeu, C. D. Voinescu, and S. Fazli, "Bristle-sensors - Low-cost flexible passive dry EEG electrodes for neurofeedback and BCI applications," *Journal of Neural Engineering*, vol. 8, no. 2, p. 25008, Mar. 2011, doi: 10.1088/1741-2560/8/2/025008.
- [22] Y. M. Chi, Y. Te Wang, Y. Wang, C. Maier, T. P. Jung, and G. Cauwenberghs, "Dry and noncontact EEG sensors for mobile brain-computer interfaces," *IEEE Transactions on Neural Systems and Rehabilitation Engineering*, vol. 20, no. 2, pp. 228–235, Mar. 2012, doi: 10.1109/TNSRE.2011.2174652.
- [23] L. F. Wang, J. Q. Liu, B. Yang, and C. S. Yang, "PDMS-based low cost flexible dry electrode for long-term EEG measurement," *IEEE Sensors Journal*, vol. 12, no. 9, pp. 2898–2904, Sep. 2012, doi: 10.1109/JSEN.2012.2204339.
- [24] Y. J. Huang, C. Y. Wu, A. M. K. Wong, and B. S. Lin, "Novel active comb-shaped dry electrode for eeg measurement in Hairy site," *IEEE Transactions on Biomedical Engineering*, vol. 62, no. 1, pp. 256–263, Jan. 2015, doi: 10.1109/TBME.2014.2347318.
- [25] M. Maqsood, S. A. Lashari, M. A. Saare, S. A. Sari, Y. M. Hussein, and H. O. Hatem, "Minimization Response Time Task scheduling Algorithm," *IOP Conference Series: Materials Science and Engineering*, vol. 705, no. 1, p. 12008, Nov. 2019, doi: 10.1088/1757-899X/705/1/012008.
- [26] N. H. Liu, C. Y. Chiang, and H. M. Hsu, "Improving driver alertness through music selection using a mobile EEG to detect brainwaves," *Sensors (Switzerland)*, vol. 13, no. 7, pp. 8199–8221, 2013, doi: 10.3390/s130708199.
- [27] J. B. F. Van Erp, F. Lotte, and M. Tangermann, "Brain-computer interfaces: Beyond medical applications," *Computer*, vol. 45, no. 4, pp. 26–34, Apr. 2012, doi: 10.1109/MC.2012.107.
- [28] B. J. Lance, S. E. Kerick, A. J. Ries, K. S. Oie, and K. McDowell, "Brain-computer interface technologies in the coming decades," *Proceedings of the IEEE*, vol. 100, no. SPL CONTENT, pp. 1585–1599, May 2012, doi: 10.1109/JPROC.2012.2184830.
- [29] P. Aspinall, P. Mavros, R. Coyne, and J. Roe, "The urban brain: Analysing outdoor physical activity with mobile EEG," *British Journal of Sports Medicine*, vol. 49, no. 4, pp. 272–276, Mar. 2015, doi: 10.1136/bjsports-2012-091877.
- [30] Z. Wen, R. Xu, and J. Du, "A novel convolutional neural networks for emotion recognition based on EEG signal," in *2017 International Conference on Security, Pattern Analysis, and Cybernetics, SPAC 2017*, Dec. 2018, vol. 2018-January, pp. 672–677. doi: 10.1109/SPAC.2017.8304360.
- [31] L. Kumar and K. K. Bharti, "An improved BPSO algorithm for feature selection," in *Lecture Notes in Electrical Engineering*, vol. 524, Springer Singapore, 2019, pp. 505–513. doi: 10.1007/978-981-13-2685-1_48.
- [32] S. Mirjalili, "Moth-flame optimization algorithm: A novel nature-inspired heuristic paradigm," *Knowledge-Based Systems*, vol. 89,

pp. 228–249, Nov. 2015, doi: 10.1016/j.knosys.2015.07.006.




- [33] W. L. Zheng and B. L. Lu, "Investigating critical frequency bands and channels for EEG-based emotion recognition with deep neural networks," *IEEE Transactions on Autonomous Mental Development*, vol. 7, no. 3, pp. 162–175, Sep. 2015, doi: 10.1109/TAMD.2015.2431497.

BIOGRAPHIES OF AUTHORS






Tabarek Alwan Tuab    was born in sammawah, Iraq, in 1996. He received a B.S in computer techniques/computer electronics engineering in 2017-2018 from the Electrical Engineering Technical College and an M.S. degree in Computer Engineering, Artificial Intelligence, and Robotics from Islamic Azad University, in 2021, respectively. She studies a Ph.D. degree in Computer Engineering, Artificial Intelligence in University of Tabriz. Her current research interests include deep learning, machine learning, artificial intelligence. She can be contacted at email: tabarcka@gmail.com.






Baydaa Hadi Saoudi    was born in sammawah, Iraq, in 1970. She received a B.S. in Computer Science in 1990-1991 from Technology University Baghdad City. I am studying for a master's degree in Artificial Intelligence in Iran from Isfahan Azad University. She can be contacted at email: ins.byd44@atu.edu.iq.






Yaqhdhan Mahmood Hussein    was born in sammawah, Iraq, in 1991. He received the B.S in computer techniques engineering in 2014-2015 from Islamic University College in Najaf city. and M.S. degrees in Electronic Engineering (Telecommunication System) from University Technical Malaysia Melaka, Malaysia, in 2018, respectively. He studies the Ph.D. degree in Electronic Engineering in University Technology Malaysia in Johor Bahru city, His current research interests include millimeter wave antennas, base station antennas, and SIW technology with butler matrix and beamforming. He can be contacted at email: Yaqthanm79@gmail.com.



Thulfiqar H. Mandeel    was born in Iraq in 1991. He received the M.Sc. degree in Embedded System Design Engineering and Ph.D. degree in Computer Engineering from Universiti Malaysia Perlis (UniMAP) in Perlis, Malaysia in 2015 and 2019 respectively. He joined UniMAP in 2016 as a graduate assistant, and is currently a lecturer in Imam Ja'afar Al Sadiq University in Iraq. His current research interests include image processing, biometric recognition, medical image classification, and deep learning. He can be contacted at email: Thulfiqar.hussein@sadiq.edu.iq.



Fahad Taha Al-Dhief    was born in Iraq, Amarah city. He received the B.S. in Software Engineering from Imam Jaafar Al-Sadiq University, Iraq in 2013 and also received M.S. in Computer Science from University Kebangsaan Malaysia, Malaysia in 2016. Currently, he is a Ph.D. student at Universiti Teknologi Malaysia, Faculty of Electrical Engineering, Department of Communication Engineering, Malaysia. He is an active student member of IEEE, and a member of IEEE Communications Society. His research interests are sensor network, routing protocols, mobile ad-hoc network, social network, internet of things, machine learning, artificial neural networks, deep learning, and location-based service. He can be contacted at email: Taha-1989@graduat.utm.my.